

BRIEF REPORT

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# Electric impedance tomography-guided PEEP titration reduces mechanical power in ARDS: a randomized crossover pilot trial

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## Abstract

**Background** In patients with acute respiratory distress syndrome undergoing mechanical ventilation, positive end-expiratory pressure (PEEP) can lead to recruitment or overdistension. Current strategies utilized for PEEP titration do not permit the distinction. Electric impedance tomography (EIT) detects and quantifies the presence of both collapse and overdistension. We investigated whether using EIT-guided PEEP titration leads to decreased mechanical power compared to high-PEEP/FiO<sub>2</sub> tables.

**Methods** A single-center, randomized crossover pilot trial comparing EIT-guided PEEP selection versus PEEP selection using the High-PEEP/FiO<sub>2</sub> table in patients with moderate–severe acute respiratory distress syndrome. The primary outcome was the change in mechanical power after each PEEP selection strategy. Secondary outcomes included changes in the 4 × driving pressure + respiratory rate (4 ΔP, + RR index) index, driving pressure, plateau pressure, PaO<sub>2</sub>/FiO<sub>2</sub> ratio, and static compliance.

**Results** EIT was consistently associated with a decrease in mechanical power compared to PEEP/FiO<sub>2</sub> tables (mean difference − 4.36 J/min, 95% CI − 6.7, − 1.95,  $p=0.002$ ) and led to lower values in the 4ΔP + RR index (− 11.42 J/min, 95% CI − 19.01, − 3.82,  $p=0.007$ ) mainly driven by a decrease in the elastic–dynamic power (− 1.61 J/min, − 2.99, − 0.22,  $p=0.027$ ). The elastic–static and resistive powers were unchanged. Similarly, EIT led to a statistically significant change in set PEEP (− 2 cmH<sub>2</sub>O,  $p=0.046$ ), driving pressure, (− 2.92 cmH<sub>2</sub>O,  $p=0.003$ ), peak pressure (− 6.25 cmH<sub>2</sub>O,  $p=0.003$ ), plateau pressure (− 4.53 cmH<sub>2</sub>O,  $p=0.006$ ), and static respiratory system compliance (+ 7.93 ml/cmH<sub>2</sub>O,  $p=0.008$ ).

**Conclusions** In patients with moderate–severe acute respiratory distress syndrome, EIT-guided PEEP titration reduces mechanical power mainly through a reduction in elastic–dynamic power.

*Trial registration* This trial was prospectively registered on Clinicaltrials.gov (NCT 03793842) on January 4th, 2019.

**Keywords** Acute lung injury, Electrical impedance tomography, Respiratory distress syndrome, Mechanical ventilators, Ventilator-induced lung injury

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### Introduction

In acute respiratory distress syndrome (ARDS) management, positive end-expiratory pressure (PEEP) counteracts gravity-dependent alveolar collapse, decreasing shunt and hypoxemia [1], reduces the shearing forces of cyclic alveolar opening/closing, and increases compliance [2]. Due to the heterogeneity of lung injury in ARDS, the application of PEEP can result in recruitment in some lung areas while causing overdistension in others. Sub-optimal PEEP may induce ventilator-induced lung injury (VILI) [1].

Randomized controlled trials (RCTs) comparing high vs. low PEEP strategies have not consistently demonstrated the superiority of either [3]. While a network meta-analysis of 18 RCTs suggested a potential mortality benefit of higher PEEP [4], this cumulative analysis failed to consider the impact of individualized PEEP titration and the adverse effects of high PEEP on non-PEEP responders [5].

Electric impedance tomography (EIT) is a bedside imaging technique that identifies changes in lung impedance, a proxy for lung volume [6]. EIT-guided PEEP titration distinguishes PEEP-induced recruitment from overdistension [7–9]. Hse et al. demonstrated increased survival with EIT-guided PEEP titration, albeit with higher use of ECMO in the EIT group [10]. Another RCT failed to demonstrate such benefit [11].

Mechanical power (MP) is a physiological construct of the energy transmitted to the patient during invasive mechanical ventilation (IMV). MP integrates the major components of positive pressure ventilation that drive VILI [12]: elastic–static (related to PEEP), elastic–dynamic (related to driving pressure,  $\Delta P$ ), and resistive (related to flow and airway resistance). High MP is associated with ARDS mortality [13]. Given the conflicting data regarding the utility of EIT and the need for feasible surrogate endpoints to guide larger multicenter RCT, we performed a randomized crossover trial to explore the effects of EIT-guided PEEP titration on MP in patients with ARDS. We hypothesized that EIT-guided PEEP titration would result in lower MP, compared to the use of the High-PEEP/ $\text{FiO}_2$  table.

### Materials and methods

#### Study design and population

In this single-center randomized crossover trial, we compared EIT-guided PEEP selection vs. High-PEEP/ $\text{FiO}_2$  tables (NCT 03793842). The University of Michigan Institutional Review Board approved this study (HUM00148126). We obtained informed consent from each patient’s legal representative. We included patients  $\geq 18$  years receiving IMV for ARDS

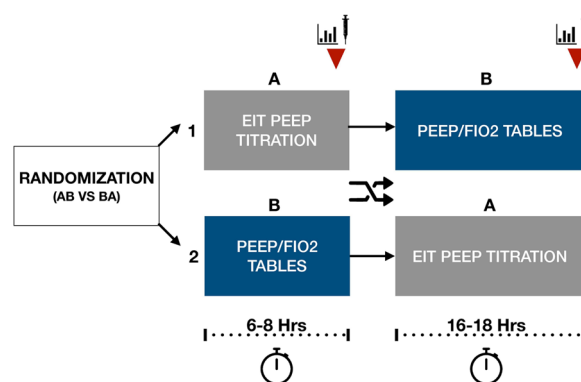
management for  $< 72$  h with a  $\text{PaO}_2/\text{FiO}_2$  ratio  $< 150$  and a PEEP  $> 8$   $\text{cm}/\text{H}_2\text{O}$ . Exclusion criteria are provided in Additional file 1.

#### Study protocol

Patients were randomly assigned 1:1 to receive EIT-guided PEEP titration followed by PEEP selection via the High-PEEP/ $\text{FiO}_2$  table (EIT first) or vice versa (tables first). Randomization was achieved using opaque, sealed envelopes. At randomization, all patients received lung-protective ventilation (LPV). PEEP was selected according to High-PEEP/ $\text{FiO}_2$  tables. Due to the need to maintain PEEP, a washout period was not feasible. Patients who were prone after randomization were excluded from the analysis due to its effects on PEEP requirement and MP [14].

During the EIT-guided PEEP titration phase, patients underwent a recruitment maneuver. PEEP was then decreased by two  $\text{cmH}_2\text{O}$  every 5–10 min until a 10% drop in delta end-expiratory lung impedance in dorsal regions was detected by EIT, five  $\text{cmH}_2\text{O}$  PEEP was reached, or hemodynamic instability/hypoxemia developed. PEEP was then set based on the intercept between the lower overdistension and collapse percentages [15].

Patients randomized to the EIT-first group underwent EIT-guided PEEP titration, as above. This was followed by six hours of management per the University of Michigan ARDS protocol (Additional file 1), with PEEP left at the EIT-determined level. Afterward, patients crossed over to a PEEP level set using the High-PEEP/ $\text{FiO}_2$  tables, which was maintained for 14–18 h. Patients randomized to the tables-first group underwent the same interventions in the reverse order (Fig. 1). After both interventions,  $\text{FiO}_2$  and respiratory rate (RR) were adjusted for oxygenation  $> 90\%$  and a pH 7.3–7.45, respectively.



**Fig. 1** Trial design and crossover. Red arrows represent the time point at which post-intervention data were collected. Center crossed arrows represent the time of crossover

## Outcomes

The primary outcome of this study was the change in MP after each PEEP selection strategy. Secondary outcomes included changes in the  $4\Delta P + RR$  index (an estimate of ventilator energy transfer to the lung) [13], elastic–static, elastic–dynamic, and resistive powers, as well as  $\Delta P$ , plateau pressure (Pplat),  $PaO_2/FiO_2$  ratio, and static compliance (Cstat). We calculated MP with Gattinoni's simplified formula:  $0.098 \times RR \times TV (P_{peak} - [P_{plat} - PEEP/2])$  [12] and analyzed its components.

## Statistical analysis

We compared baseline characteristics using Fisher's test for categorical and a two-sample *t* test for continuous variables. Changes in ventilator parameters with each intervention were compared using paired *t* tests. We fit serial linear mixed-effect regression models assessing the association between the interventions and change in MP, adjusting for randomization order and pre-intervention MP in sequential models. We repeated this to determine the association between intervention and the  $4\Delta P + RR$  index, MP components, and  $\Delta P$ . Our small sample size represents a convenience sample similar in scope to other EIT studies. Statistical analyses were performed in StataMP version 17.0 (StataCorp).

## Results

Sixteen patients were enrolled in this study. One patient was withdrawn due to hemodynamic instability; three were prone after randomization and excluded from the analysis (Additional file 2: Fig S1). Baseline characteristics are shown in Table 1. The median baseline MP was 20 J/min (IQR: 19, 28). EIT led to a significant change in PEEP compared to tables (mean difference of change:  $-2$  cmH<sub>2</sub>O, 95% CI  $-3.95, -0.05$ ,  $p=0.046$ ),

EIT decreased MP compared to PEEP/ $FiO_2$  tables ( $-4.36$  J/min, 95% CI  $-6.7, -1.95$ ,  $p=0.002$ ). (Table 2). This difference persisted after adjusting for randomization order and pre-intervention MP. (Additional file 3: Tables S1-2). EIT led to a decrease in the  $4\Delta P + RR$  index ( $-11.42$  J/min, 95% CI  $-19.01, -3.82$ ,  $p=0.007$ ) mainly through a decrease in elastic–dynamic power ( $-1.61$  J/min, 95% CI:  $-2.99, -0.22$ ,  $p=0.027$ ), and driving pressure ( $-2.92$  J/min, 95% CI:  $-4.59, -1.23$ ,  $p=0.003$ ) (Table 2 and Fig. 2). These differences persisted after adjusting for randomization order and baseline MP (Additional file 3: Table S3). Elastic–static and resistive powers were unchanged across both interventions.

EIT led to changes in peak pressures ( $-6.25$  cmH<sub>2</sub>O,  $p=0.003$ ), Pplat ( $-4.53$  cmH<sub>2</sub>O,  $p=0.006$ ), and Cstat

( $+7.93$  ml/cmH<sub>2</sub>O,  $p=0.008$ ) (Additional file 4: Fig S2). There was no significant change in RR or  $PaO_2/FiO_2$  ratio.

After the EIT phase, one patient developed pneumomediastinum, which did not require additional intervention. Three patients developed hypotension during the RM. In one patient, the protocol was stopped due to persistent hemodynamic instability.

## Discussion

In this randomized crossover trial, we found a significant decrease in MP using EIT-guided PEEP titration compared to High-PEEP/ $FiO_2$  tables in mechanically ventilated patients with moderate–severe ARDS. This difference persisted after sensitivity analysis and adjustment for randomization order and pre-intervention MP. A reduction in the elastic–dynamic MP mainly drove the decrease in MP.

Zhao and colleagues reported that EIT-guided PEEP titration was associated with improved respiratory mechanics [15]. Similarly, a RCT by Hsu and colleagues reported improvement in  $\Delta P$ , Cstat, and survival rates with EIT-guided PEEP titration compared to the pressure–volume curves through a decrease in PEEP [11].

He and colleagues compared the effects of EIT-guided PEEP titration vs. a low PEEP/ $FiO_2$  table [10] without finding differences in survival, ventilator-free days, or ICU stay. However, this study was limited by using similar PEEP between groups and including mild ARDS. In our study, EIT-guided PEEP titration led to significant changes in PEEP, and we only enrolled patients with moderate–severe ARDS. Using a crossover design allowed us to analyze the effects of each intervention on an individual level by using each patient as their own control. Using the High-PEEP/ $FiO_2$  tables as the control intervention permitted comparison with the strategy associated with better ventilation/perfusion matching [16] and outcomes in severe ARDS [4].

In patients with ARDS, persistent elevation of MP  $>17$  J/min is associated with higher mortality [13, 17]. Although patients in our study received standard LPV per protocol at baseline, MP was elevated (median 20 J/min). EIT-guided PEEP titration led to a mean reduction of MP by 4.36 J/min, a reduction associated with decreased mortality [17, 18], particularly when achieved during the initial hours of IMV [18]. The reduction in MP was achieved through decreased elastic–dynamic power, but not the elastic–static or resistive powers. Although changes in RR were allowed to achieve  $pH > 7.3$ , they were not different across groups.

Our findings are consistent with previous observations [13] that propose oscillating mechanical stresses as the main injurious mechanism for VILI. In our study,

**Table 1** Baseline characteristics of participants across study arms

	All (n = 12)	EIT first (n = 6)	Tables first (n = 6)
Age, median [IQR], years	61 [48, 68]	62 [50, 72]	59.5 [46, 67]
Female sex, n(%)	3 (25)	1 (16)	2 (33)
White race, n(%)	11 (91)	6 (100)	5 (83)
BMI, median [IQR], kg/m <sup>2</sup>	32 [25, 36]	32 [26, 36]	32 [24, 36]
CCI, median [IQR]	2 (1, 5)	2 (1, 5)	2.5 (1, 5)
Tobacco Use, n(%)	9 (75)	4 (66)	5 (83)
SAPS II at ICU admission, median [IQR]	38 [33, 46]	38 [33, 45]	40 [33, 48]
SOFA at ICU admission, median [IQR]	8 (6, 9)	7 (6, 9)	8.5 (7, 10)
<i>Etiology of ARDS, n(%)</i>			
COVID-19	7 (58.3)	4 (66.7)	3 (50.0)
Bacterial pneumonia	4 (33.3)	2 (33.3)	2 (33.3)
Extrapulmonary	1 (8.3)	0 (0)	1 (16.7)
Pre-intubation NIV and/or HFNC, n(%)	11 (91.7)	6 (100)	5 (83.3)
PaO <sub>2</sub> /FiO <sub>2</sub> Ratio, median [IQR], mmHg	130 [112, 140]	117 [111, 143]	136 [125, 138]
MV duration before inclusion, median [IQR], days	0.6 [0.2, 2]	0.5 [0.2, 2]	1 [0.2, 1]
Vasopressor at baseline, n(%)	9 (75)	5 (83.3)	4 (66.7)
Sedation at baseline (RASS), median [IQR]	- 4 [- 3, - 4.5]	- 4 [- 3, - 5]	- 3.5 [- 3, - 4]
<i>Baseline Ventilator Settings*, median [IQR]</i>			
Tidal Volume, ml/kg/PBW	6.0 [5.9, 6.3]	6.1 [5.7, 6.3]	6.0 [5.8, 6.3]
Respiratory rate, breaths/min	26 [20, 30]	26 [21, 30]	26 [20, 31]
PEEP, cmH <sub>2</sub> O	15 (14, 16)	14 (14, 16)	16 (14, 16)
Cstat, ml/cmH <sub>2</sub> O	36 [29, 40]	34 [28, 39]	36 [32, 42]
Ppeak, cmH <sub>2</sub> O	27 [25, 31]	29 [27, 35]	25 [25, 27]
Pplat, cmH <sub>2</sub> O	26 [25, 28]	27 [26, 28]	26 [25, 27]
Driving Pressure, cmH <sub>2</sub> O	11 (10, 12)	12 (12, 14)	10 (10, 11)
Mechanical Power <sup>†</sup> , J/min	20 [19, 28]	24 [20, 35]	19 [18, 22]
4ΔPxRR Index <sup>‡</sup> , J/min	70 [64, 83]	76 [68, 84]	70 [60, 73]
Non-Survivors, n(%)	6 (50)	3 (50)	3 (50)

\*Baseline ventilator settings are defined as ventilator settings at the start of the study, after randomization but prior to initiation of any study intervention

<sup>†</sup> Mechanical Power calculate using Gattinoni's simplified equation

<sup>‡</sup> Mechanical Power calculated using 4ΔPxRR index

EIT electrical impedance tomography, IQR interquartile range, SD standard deviation, BMI body mass index, CCI Charlson Comorbidity Index, Tobacco use ever tobacco user (current and former smokers), SAPS II Simplified Acute Physiology Score II, ICU intensive care unit, SOFA Sequential Organ Failure Assessment, ARDS acute respiratory distress syndrome, COVID-19 coronavirus disease 2019, MV mechanical ventilation, NIV noninvasive ventilation, HFNC high flow nasal cannula, PaO<sub>2</sub> partial pressure of oxygen, FiO<sub>2</sub> fraction of inspired oxygen, RASS Richmond Agitation Sedation Scale, MV mechanical ventilation, min minute, PBW predicted body weight, PEEP positive end-expiratory pressure, Cstat static respiratory system compliance, Ppeak peak pressure, Pplat plateau pressure, J joules

EIT decreased PEEP levels despite ΔPs believed to be LPV, suggesting EIT-directed PEEP titration to be a more effective means of optimizing LPV than PEEP/FiO<sub>2</sub> tables via a reduction in MP. In addition, observational studies have shown that lung recruitment is not systematically associated with detectable improvements in Cstat nor ΔP, therefore precluding accurate titration of PEEP based exclusively on these parameters [19, 20].

Our study has several limitations; 1) excluding subjects on prone positioning could have introduced post-randomization selection bias. 2) Sample was small, but the effects in MP reduction were significant and

occurred despite optimal LPV at baseline. This suggests a strong effect of EIT in reducing MP. 3) We did not include a washout phase. However, our analysis considered the order of interventions to assess for carryover effects. 4) We did not assess for recruitability before the recruitment maneuver. This could have impacted sample's enrichment. 5) Our intervention focused on titrating PEEP during the initial 24 h. However, PEEP/FiO<sub>2</sub> tables are meant to guide continuous changes in PEEP based on FiO<sub>2</sub> responses, dead space fraction, and mechanics. This was not assessed. 6) MP was calculated using airway not transpulmonary ΔP rather which could have introduced measurement bias.

**Table 2** Comparison of changes in ventilator parameters with EIT vs tables, for all participants,  $n = 12$

	Change with EIT*	Change with tables**		95% CI of mean difference	<i>p</i> value
Mechanical Power <sup>1</sup> , J/min	- 2.50 ± 3.70	1.87 ± 1.61	- 4.36	(- 6.77, - 1.95)	0.002
4ΔP + RR Index, J/min	- 6.80 ± 9.36	4.62 ± 6.25	- 11.42	(- 19.01, - 3.82)	0.007
Elastic-static power <sup>2</sup> , J/min	- 1.37 ± 2.11	0.19 ± 2.28	- 1.56	(- 3.71, 0.58)	0.138
Elastic-dynamic power <sup>3</sup> , J/min	- 1.13 ± 1.66	0.48 ± 0.88	- 1.61	(- 2.99, - 0.22)	0.027
Resistive power <sup>4</sup> , J/min	0.01 ± 3.30	1.15 ± 2.48	- 1.14	(- 4.59, 2.30)	0.48
Driving Pressure, cmH <sub>2</sub> O	- 1.58 ± 2.32	1.34 ± 1.31	- 2.92	(- 4.59, - 1.24)	0.003
PEEP (set), cmH <sub>2</sub> O	- 1.17 ± 1.80	0.83 ± 1.80	- 2	(- 3.95, - 0.05)	0.046
Ppeak, cmH <sub>2</sub> O	- 2.75 ± 3.55	3.5 ± 2.78	- 6.25	(- 9.79, - 2.71)	0.003
Pplat, cmH <sub>2</sub> O	- 2.48 ± 3.22	2.06 ± 1.88	- 4.53	(- 7.45, - 1.62)	0.006
RR, breaths/min	- 0.5 ± 2.35	- 0.75 ± 2.73	0.25	(- 2.71, 3.21)	0.856
Cstat, ml/cmH <sub>2</sub> O	3.24 ± 9.85	- 4.6 ± 5.26	7.93	(2.54, 13.32)	0.008
PaO <sub>2</sub> /FIO <sub>2</sub> ratio	25.14 ± 27.11	- 0.89 ± 60.05	26.03	(- 16.01, 68.06)	0.2

Data are listed as mean ± SD

*P* value calculated using paired *t* test

\*Change with EIT: ventilator parameter at the end of EIT intervention minus ventilator parameter at the start of the EIT intervention

\*\*Change with tables: ventilator parameter at the end of the table intervention minus ventilator parameter at the start of the table intervention

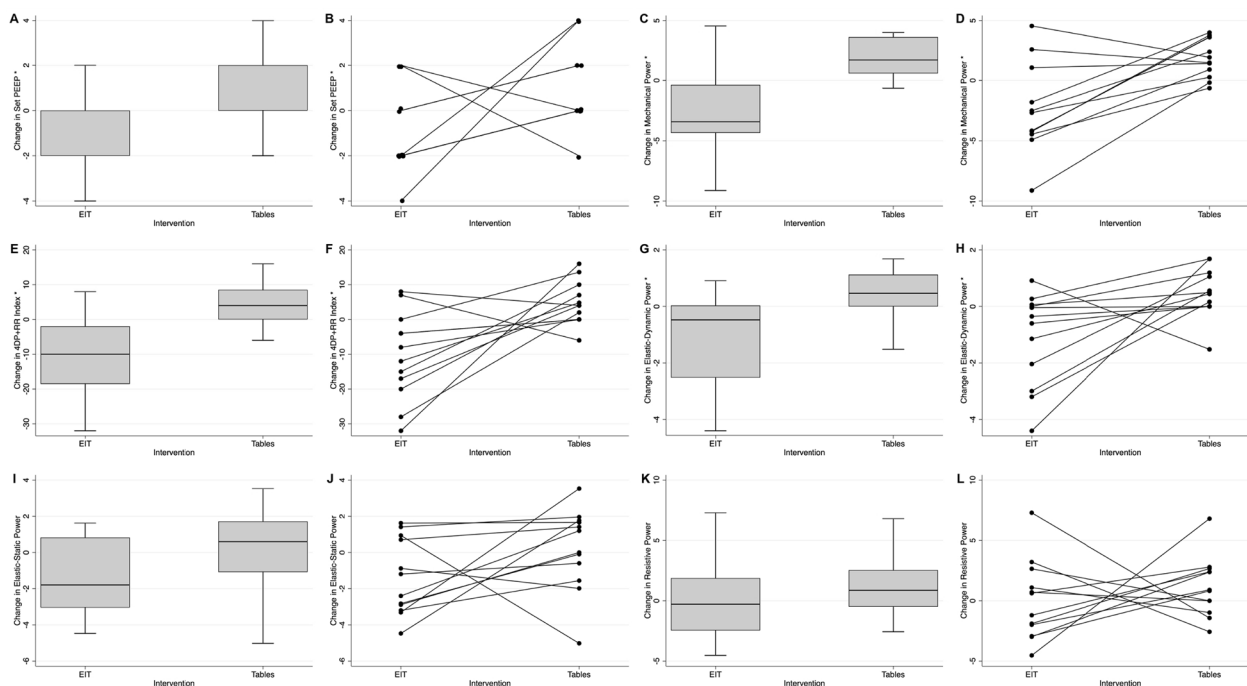
<sup>1</sup> Mechanical Power calculate using Gattinoni’s simplified equation

<sup>2</sup> Elastic-static power, related to PEEP (J/min) = 0.098 \* VT \* RR \* PEEP

<sup>3</sup> Elastic-dynamic power, related to DP (J/min) = 0.0983 \* VT \* RR \* 0.5 \* DP

<sup>4</sup> Resistive power, related to resistance in the ventilator circuit, endotracheal tube, and airways (J/min) = 0.098 \* VT \* RR \* (Ppeak—Pplat)

EIT Electrical Impedance Topography, *J* joules, *min* minute, PEEP positive end-expiratory pressure, Ppeak peak pressure, Pplat plateau pressure, RR respiratory rate, Cstat static respiratory system compliance, PaO<sub>2</sub> partial pressure of oxygen, FIO<sub>2</sub> fraction of inspired oxygen, SD = standard deviation



**Fig. 2** Changes in mechanical power and its components after each intervention. Changes in PEEP (**A** and **B**), MP by the Gattinoni’s Simplified formula (**C** and **D**), 4ΔP×RR index (**E** and **F**), elastic-dynamic power (**G** and **H**), elastic-static power (**I** and **J**), and resistive power (**K** and **L**). Asterisk indicates a statistically significant difference in the change with the EIT versus High-PEEP tables interventions based on *p* value < 0.05

## Conclusion

This study shows that EIT-guided PEEP titration decreases MP in patients with moderate–severe ARDS compared to a high-PEEP/FiO<sub>2</sub> table. A decrease in the dynamic–elastic component primarily drives the reduction in MP. The clinical impact of EIT-guided PEEP titration should be tested in large multicenter trials.

## Abbreviations

ARDS	Acute respiratory distress syndrome
Cstat	Static compliance
EIT	Electric impedance tomography
FiO <sub>2</sub>	Fraction of inspired oxygen
IMV	Invasive mechanical ventilation
MP	Mechanical power
PEEP	Positive end-expiratory pressure
P <sub>peak</sub>	Peak pressure
P <sub>plat</sub>	Plateau pressure
RCTs	Randomized controlled trials
RR	Respiratory rate
TV	Tidal volume
VILI	Ventilator-induced lung injury
ΔP	Driving pressure

## Supplementary Information

The online version contains supplementary material available at <https://doi.org/10.1186/s13054-023-04315-x>.

**Additional file 1.** Extended methods and protocol.

**Additional file 2.** Flow diagram of the study.

**Additional file 3.** Comparison of ventilator parameters.

**Additional file 4.** Changes in respiratory mechanics.

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Not applicable

## Author contributions

JVJ, TS, and RH were involved in the study design and conception. JVJ, EM, AW, KF, and CC were involved in data acquisition. JVJ, EM, and HP performed the statistical analysis. JVJ, EM, HP, and RH analyzed and interpreted the data. JVJ drafted the manuscript. EM, AW, CC, KF, WWL, PC, IV, HP, and RH provided critical manuscript reviews. All authors participated in the final manuscript revision and take responsibility for the data's integrity and the data analysis's accuracy.

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## Availability of data and materials

The datasets used and analyzed in this study are available from the corresponding author upon reasonable request.

## Declarations

### Ethics approval and consent to participate

The Institutional Review Board of the University of Michigan approved this study (HUM00148126). We obtained informed consent from each patient's legal representative.

### Consent for publication

Not applicable.

## Competing interests

EM was supported by Grant Number T32 HL 007749 (Multidisciplinary Training Program in Lung Disease) from the National Institutes of Health. The content is solely the responsibility of the authors and does not necessarily represent the official views of the National Institutes of Health. AW reports speaking fees from Dräger and author fees from Jones and Bartlett Learning, unrelated to this work. WWL reports personal fees from Konica Minolta and Continuing Education Alliance. PC is a consultant for Breas Medical US and performs Medicolegal Expert witness work. HP reported receiving grants from the US Department of Veterans Affairs outside the submitted work, serving on the Surviving Sepsis Campaign Guidelines Panel, and serving as physician lead for a Michigan statewide sepsis collaborative. RH serves on the advisory board for Merck, Boehringer Ingelheim. Consultant for LungPacer and NOTA-Laboratories has textbook royalties from Springer Website and UpToDate. Grants: CHEST Foundation, NHLBI PETAL Network Medicolegal Expert witness work. Dräger loaned equipment (PulmoVista® 500) to RH for research purposes; no monetary funds were provided.

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